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# Development and Evaluation of Temperature Mediated In-Situ Mucoadhesive Gel of Lamotrigine for Intranasal Administration

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# **ABSTRACT**

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**Introduction:** Epilepsy a neurodegenerative disease causes spontaneous and repetitive seizures. Treatment requires instantaneous pharmacotherapy to prevent further the condition of status epilepticus.

**Aim:** The present study was aimed at developing temperature-sensitive in situ gel for intranasal administration of lamotrigine, an anticonvulsant drug used to treat generalised and partial seizure.

**Methodology:** Pluronic 127, chitosan and β-glycerophosphate were used for the preparation of gel in varying concentrations by cold method. These systems were characterized for physical properties such as pH, gelling temperature, gelling time, drug content, in vitro drug diffusion studies, ex-vivo drug permeation and histopathological studies. The drug polymer compatibility was studied using Fourier transform infrared spectroscopy.

**Results:** All the prepared formulations gelled immediately below 25 sec at the nasal pH and temperature. Addition of chitosan with Pluronic 127 increases the mucoadhesion and contact time of formulation in nasal cavity. The result of in-vitro drug release study revealed 93% of Lamotrigine and 75.33% of drug release in ex-vivo permeability study from the optimized formulation in about 210 min. Result of histopathological studies suggests the suitability of prepared formulation for intranasal administration.

**Conclusion:** In-situ intranasal gel of lamotrigine prepared by using Pluronic 127 and chitosan demonstrated gelation at body temperature and exhibited satisfactory release of drug from its dosage form. It can be concluded that the prepared formulation has potential for the intranasal administration of lamotrigine in the treatment of epilepsy.

Key Words: In-situ gel, Mucoadhesive, Intranasal administration, Lamotrigine, Temperature-sensitive, Epilepsy

#### INTRODUCTION

Epilepsy is a neurological disorder of brain characterized by sudden recurrent episodes of sensory disturbances causing seizures. Increased and unusual nerve cell activity in the cortex of the brain results in epileptic seizures.<sup>1</sup> Some occur as a result of tumour of brain, brain injury and brain defect stroke.<sup>2</sup> About 3-10 per 1000 people have epilepsy worldwide.<sup>3</sup> Selection of AED for a patient depends upon the affected individual's condition and side effects of drug.<sup>4</sup> The nasal mucosa is highly vascularised responsible for the transfer of drug through the mucus layer leads to the absorption.<sup>5</sup> A drug molecule can be transferred quickly across the single epithelial cell layer directly to the systemic blood cir-

culation without first-pass hepatic and intestinal metabolism. Nowadays nasal delivery has been focused as an alternative route of drug administration. The advantages of the nasal administration include rapid absorption, higher bioavailability, fast onset of therapeutic action, avoidance of presystemic metabolism, non-invasive administration and improved patient compliance. The poor bioavailability and therapeutic response exhibited by the conventional nasal solution due to short residence time is the basic problem of highly efficient nasal route. Mucoadhesive in situ gelling formulation is one of the approaches to enhance the residence time of the drug in the nasal cavity leading to improved drug absorption and its therapeutic effect with rapid onset of action. Mucoadhesive system aims in targeting and localization of the dosage

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forms and provide an intimate contact between dosage form and absorptive mucosa resulting in high retention time and greater absorption of drug.<sup>7,8</sup>

In situ liquid polymeric formulations once administered undergo in situ gelation. Various approaches used for in situ gelling system include physiological stimuli, osmotic stimuli, chemical stimuli, pH-triggered system, and temperature-dependent system. Temperature is most widely used stimulus in environmentally responsive polymer system. In these systems, gelling of the solution is triggered by change in temperature. These hydrogels are liquid at room temperature (20–25°C) and undergo gelation with increase in temperature when in contact with body fluid (35–37°C). The polymers which show temperature-induced gelation include chitosan, pluronics, tetronics, xyloglucans, and hydroxyl propyl methyl cellulose. 11

Lamotrigine, an antiepileptic drug regularly used to treat partial seizures and tonic-clonic convulsions. <sup>12</sup> Lamotrigine has relatively few side-effects and does not require therapeutic drug monitoring. Lamotrigine is available as tablet and intravenous formulation. In view of the potential pharmacological application of lamotrigine in the treatment of epilepsy, the present work was designed to formulate its mucoadhesive temperature-sensitive *in situ* gel for treating acute and emergency epileptic condition.

## **MATERIAL AND METHODS**

#### **Materials**

Lamotrigine was obtained as a generous gift sample from Lupin pharma, Pune, India. Chitosan, pluronic127,  $\beta$ -glycerophosphate, benzalkonium chloride were purchased from Sigma Drug Laboratory Pvt. Ltd. All the chemicals used in experiments were of analytical grade.

#### **Methods**

#### Formulation of In-Situ Gel

Table 1 depicts the concentration of lamotrigine, chitosan and pluronic F 127 used for the preparation of various batches of formulations. The concentration of Pluronic F127 was selected based on initial studies so as to obtain gel at minimum possible concentration below  $34^{\circ}$ C and pH of 4.8. Chitosan was used as mucoadhesive polymer to increase the gel strength. Benzalkonium chloride was added as preservative and β-glycerophosphate was used as antioxidant to protect the formulation from microorganisms and oxidation. Distilled water was used as vehicle.

The gel was prepared by cold method. Initially 2% w/v chitosan solution was prepared in 0.1M HCl in ice bath, to it 10% w/v of glycerophosphate solution was added dropwise

with continues stirring. Separately, pluronic F127 solutions of different concentration was prepared and kept these solutions in ice bath for removal of foam. Further chitosan solution was added to pluronic F127 solution with continues stirring. <sup>13, 14</sup>

# **Calibration curve of Lamotrigine**

A solution of 100  $\mu$ g /ml of lamotrigine was scanned in the range of 400 to 200 nm for the determination of  $\lambda$  max. Calibration curve of lamotrigine was plotted for the concentrations 2-20  $\mu$ g/ml in phosphate buffer pH 6.6.

## **Physicochemical Characterization**

Formulated in-situ intranasal gel was critically analysed for physicochemical properties such as clarity, pH, gelation time and gelation temperature. Clarity is one of the most important characteristics features of gel formulation. All the prepared gel formulations were evaluated for clarity by visual observation against black and white background. PH of each formulation was determined by using digital pH meter which was previously calibrated using buffer of pH 4 and pH 7. The pH values were recorded immediately after preparation of gel.

Gelation temperature and gelation time of various gel preparations were determined by taking formulation equivalent to 10 mg of drug in a test tube and immersed in a water bath. Temperature of water bath was increased slowly and left to equilibrate for 5 min at each new setting. The sample was then examined for gelation, which was said to have occurred when the meniscus would no longer move upon tilting through 90°C. Gelation time was measured as the time at which gel does not flow at 37°C on immersing the solutions in a thermostatic water bath.

#### Fourier Transform Infrared Spectroscopy (FTIR)

FTIR spectra of the pure drug, physical mixture of drug with polymers were obtained using FTIR (Thermo Nicolet, Avatar 370). The samples were prepared as potassium bromide (KBr) disks on an FTIR spectrophotometer (2 mg sample in 200 mg KBr ratio) and scanned in a range 400-4000/cm as described earlier. <sup>16</sup>FTIR spectra were taken to investigate compatibility between the drug and the polymer.

#### **Differential Scanning Calorimeter (DSC)**

Differential scanning calorimetric (DSC) was used to evaluate the thermal behaviour of pure drug and physical mixture of the drug and excipients. The thermal profile of mentioned samples was recorded on DSC (Mettler Toledo DSC 822e). The thermograms were obtained by heating the microspheres at rate of 10°C/min from 30°C to 300°C using nitrogen purge of 50 ml/min.<sup>17</sup>

## X-ray Diffraction Studies (XRD)

X- ray diffractogram analysis provides information about crystalline and amorphous nature of the substances. Diffractograms were recorded for the pure drug and formulation on X-ray diffractometer (Brucker AXS D8) to evaluate its crystallinities. Diffractograms were scanned in the range from 3°C to 80°C (2θ) with resolution of 0.02°C and scanning speed of 2.0°C/min. An accelerating voltage of 40 kV was applied at the current intensity of 35 mA. The XRD pattern of in situ gel formulation was compared with that of the pure drug.<sup>4</sup>

#### **Drug Content**

Drug content of prepared formulations was determined by dissolving 1 ml gel formulation into 50 ml of pH 6.6 phosphate buffer solution. The resultant solution was analysed for the drug content by ultraviolet (UV)-visible spectrophotometer at 306 nm (Shimadzu 7800, Tokyo Japan). pH 6.6 phosphate buffer was used as blank. The data were collected by repeating the procedure in triplicate.

## In vitro drug diffusion studies

The in vitro drug diffusion study of gel formulations was carried out using Franz diffusion cell across dialysis membrane (Av diameter 21.5 mm, Av flat width 32.34 mm) as diffusion barrier. The membrane was equilibrated overnight with pH 6.6 phosphate buffer before application of gel onto the donor compartment. The receptor compartment was filled with phosphate buffer solution (pH 6.6) that was within the pH range in the nasal cavity. The donor compartment was placed in such a way that it just touched the diffusion medium in the receptor compartment. The temperature was maintained at  $37^{\circ}\text{C} \pm 1^{\circ}\text{C}$  using circulating water bath.  $300~\mu\text{l}$  of sample was withdrawn at predetermined time points from the receptor compartment, replaced with the same amount of fresh pre-warmed buffer solution and analysed for lamotrigine using UV-visible spectrophotometer at 306 nm.  $^{18}$ 

## **Ex Vivo Permeation Studies**

For the purpose of this study, fresh nasal tissue of goat was obtained from the local slaughterhouse. The nasal mucosa was separated from septum and the connective tissue as well as most of the adhering cartilaginous tissue was carefully removed with forceps and scissors without damaging or scratching the nasal mucosa. The specimen was individually placed on Franz diffusion cell and clamped between the donor and receptor compartments. 18 ml of pH 6.6 phosphate buffer was maintained at 37° was placed in the receptor compartment. Formulation equivalent to 10 mg of lamotrigine was placed in the donor compartment. Sampling was done in a similar manner as for *in vitro* release studies. The amount of lamotrigine diffused into the receptor phase from the formulations was determined by UV spectrophotometry at 306

nm. The method was found to be sensitive enough for detecting the amount of drug permeated. 18

## Ex vivo biocompatibility study

The histopathological studies were accomplished to confirm the biocompatibility of lamotrigine intranasal in-situ gel formulation with goat nasal mucosa. The freshly excised nasal mucosa of goat was collected and cleaned with saline solution as mentioned in vitro drug diffusion study. After application of predefined amounts of lamotrigine in-situ gel (1 mg), mucosal tissues were fixed in 10% formalin solution and implanted in paraffin. Paraffin sections (7.5 μm) were stained with Hematoxylin Eosin and observed under digital Motic microscope (Model no B1-223SP). The untreated mucosa incubated with phosphate buffer solution (pH 6.6) was used as a control.<sup>19</sup>

## Statistical analysis

All the results are reported as mean  $\pm$  standard deviation (SD) or mean  $\pm$  standard error mean (SEM)

#### **RESULT AND DISCUSSION**

In-situ temperature-sensitive intranasal mucoadhesive gel of lamotrigine was prepared by cold method. Initially various concentrations of Pluronic F127 were used to obtain formulation that forms gel at temperature near 34°C and pH of 4.8. Formulations showed adequate gelation in proper time at concentration of 32% w/v and 34% w/v. Chitosan concentration was also varied to obtain gel having suitable viscosity. Based on these studies' concentration of chitosan and Pluronic F127 was selected for the further formulations. The purity of lamotrigine was checked by determining the melting point of it by capillary method which was found to be  $216^{\circ}$  C  $-218^{\circ}$  C. The drug exhibited the  $\lambda$  max at 306 nm and showed reproducibility. Calibration curve of lamotrigine obeyed Beers-Lambert's law in the concentration range 2-20 µg/ml (Figure 1).

#### **Physicochemical Characterization**

All the formulations showed the pH in the range of  $4.87 \pm 0.16$  to  $5.37 \pm 0.08$ , which is suitable according to the nasal pH. All the formulations were clear in appearance in sol form. The gelling temperature of the prepared formulations were in the range  $32.23 \pm 1.87$  to  $35.30 \pm 1.22$  °C. In the present study, all the formulations showed gelation temperature within the acceptable range. The gelling temperature suitable for temperature-sensitive in-situ nasal gel ranges between 30-36 °C. The gelation point refers to the temperature when the meniscus of the formulation would no longer move upon slanting the test tubes at  $90^{\circ}$ , with gradual increase in the temperature. The gelling time of all the formulations was found in the range of  $15.06 \pm 0.90$  to  $25.33 \pm 4.48$  sec. All the

formulations exhibited satisfactory gelation time for intranasal administration for lamotrigine (Table 1).

## **Fourier Transform Infrared Spectroscopy**

FTIR spectra of lamotrigine showed characteristic absorbance at 3448 cm-1 specifying NH stretching of an amino group (Aromatic), 3209 cm-1 shows aromaticity (aromatic CH stretching), 1620 cm-1, 1486 cm-1 indicates C=C ring stretching and 962 cm-1. In FTIR spectra of physical mixture characteristics peak of both lamotrigine and excipients were observed. It suggests no significant interaction between drug and excipient. However, the characteristic absorbance peaks of lamotrigine were found to be shifted to the lower values and decreased in intensity also, suggesting the incorporation of lamotrigine within in-situ gel prepared with Pluronic F127 and chitosan as carriers (Figure 2).

# **X-ray Diffraction Studies**

The X-ray diffractogram of lamotrigine shows a sharp and intense peak indicating the crystalline nature of the drug in pure form. The X-ray diffractogram of the physical mixture was observed to determine if there is a loss or modification of the pure drug's crystal structure. Figure 3 indicates that there is virtually no difference in crystallinity between physical mixture of drug with excipients and pure lamotrigine proposed compatibility between the lamotrigine and the excipients.

# **Drug content**

Drug content of the formulations was found to increase with the increase in concentration of pluronic F 127 and chitosan. The drug content of the formulations was ranging from 48.35  $\pm 3.55\%$  to 69.12  $\pm 2.77\%$ , indicating maximum entrapment of drug in the formulation (**Table 2**). The maximum amount of drug content 69.12  $\pm 2.77\%$  was obtained for in-situ gel formulation with 34% of Pluronic F127 and 8% of chitosan concentration.

#### In vitro drug diffusion study

The release of lamotrigine from the in situ intranasal formulations was determined using Franz diffusion cell. The receptor compartment was filled with phosphate buffer pH 6.6 as the dissolution medium. In vitro drug diffusion study revealed that the release rate dependent on Pluronic F127 and chitosan concentration. Higher the pluronic F127 concentration, greater the rate of drug release was observed from the formulations. However, formulations with greater chitosan concentration decreased the rate of drug release might be due to increased viscosity of the gel formulation. With the concentration of chitosan 2% and 4%, showed the greater release of lamotrigine. Bioadhesive property of chitosan is responsible to retain the formulation at the administration site helps to increase the retention time, also increases the transmembrane permeability of drug and thereby exhibit bet-

ter absorption of the drug. The formulation F6 containing 34% w/v of Pluronic F127 and 4% w/v of chitosan concentration showed 93% of drug release in 270 min (**Figure 4**). The same formulation was selected further for the ex-vitro permeation study and histopathological study.

## **Ex-vivo permeation study**

The ex-vivo permeation study of formulations F6. Ex-vivo permeation study was performed for the significant batch using goat nasal mucosa. The percent drug permeated after 210 min was found to be 85.18±2.28% (**Figure 5**) from nasal gel formulation showing significant release of drug from the formulation.

## Ex vivo biocompatibility study

The epithelium layer was intact and there were no alterations in basal membrane and superficial part of sub mucosa as compared with PBS treated mucosa (Figure 6). Thus, insitu gel formulations seem to be safe with respect to nasal administration.

#### CONCLUSION

In this study we have formulated intranasal mucoadhesive in-situ temperature-sensitive gel of lamotrigine. Physicochemical characterization exhibited satisfactory gelation of formulation in 25 sec. In-vitro and ex-vivo drug permeation studies have shown that in situ gels act as potential drug delivery system for lamotrigine. Histopathological study revealed the safe intranasal administration of in-situ gel formulation. Present study highlighted the importance of intranasal administration of lamotrigine as mucoadhesive in-situ temperature-sensitive gel for emergency conditions of epileptic seizures. However, in vivo studies are required to be carried out to confirm the potential of these formulations.

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# **Conflict of Interest**

The author stated no conflict of interest for the publication of this research article.

Rathi Tejas- Data collection, methodology, formal analysis and investigation.

Khetade Roshan- Data collection, methodology, formal analysis and investigation.

Dhande Payal- Data collection, methodology, formal analysis and investigation.

Taksande Jayshree- Supervision, validation, writing original draft and editing.

Das Renuka- Supervision, validation, writing original draft and editing.

Umekar Milind- Supervision, validation, writing original draft and editing.

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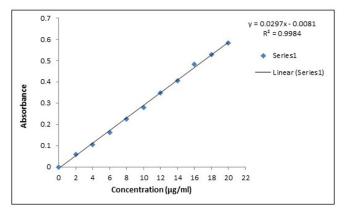
Table 1: Composition of different batches of lamotrigine loaded in-situ intranasal gel

Ingredients	F1	F2	F <sub>3</sub>	F4	F5	F6	F <sub>7</sub>	F8
Pluronic F127 (%w/v)	32	32	32	32	34	34	34	34
Chitosan (%w/v)	2	4	6	8	2	4	6	8
Lamotrigine (mg)	100	100	100	100	100	100	100	100

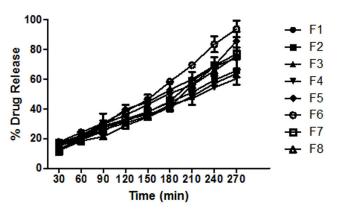
Table 2: pH, Gelling Temperature, Gelling Time and Drug Content of various in-situ gel formulations.

Formulations	pН	Gelling Temperature (C)	Gelling Time(Sec)	Drug Content(%)
F1	4.87 ±0.16	34.06 ±1.00	16.43 ±3.73	48.26 ±13.55
F2	5.24 ±0.04	35.30 ±1.22	19.83 ±5.22	50.35 ±2.98
F <sub>3</sub>	5.28 ±0.03	35.06 ±0.50	20.63 ±2.50	52.97 ±20.45
F4	5.22 ±0.04	34.00 ±1.24	18.00 ±1.99	56.39 ±32.34
F <sub>5</sub>	5.37 ±0.08	32.23 ±1.87	16.87 ±2.70	65.12 ±18.77
F6	5.13 ±0.07	33.93 ±0.41	17.26 ±0.64	67.67 ±1.24
F <sub>7</sub>	5.06 ±0.03	31.76 ±1.16	15.06 ±0.90	68.67 ±12.73
F8	5.04 ±0.03	33.26 ±0.30	17.43 ±4.36	69.22 ±30.18

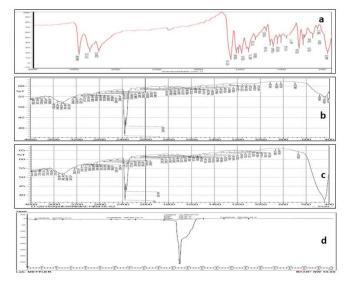
Results are shown as mean $\pm$ SD (n=3)



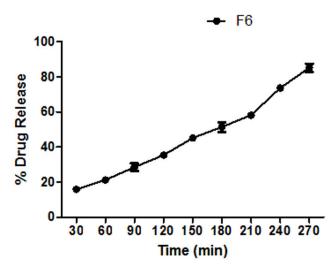
**Figure 1:** Calibration curve of lamotrigine in pH 6.6 phosphate buffer.



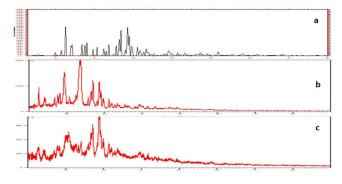
**Figure 4:** In-vitro drug diffusion study of in situ nasal gel formulations.



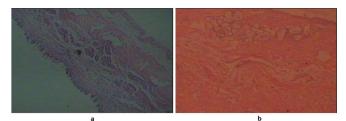
**Figure 2:** FTIR spectra: a- Lamotrigine, b- Physical mixture of lamotrigine and PF127, c- Physical mixture of lamotrigine and chitosan, d- In-situ gel Formulation.



**Figure 5:** Ex-vivo permeation of in-situ gel through nasal mucosa.



**Figure 3:** XRD: a- Lamotrigine, b- Physical mixture of lamotrigine and PF127, c- Physical mixture of lamotrigine and chitosan.



**Figure 6:** Light photomicrograph of goat nasal mucosa, A) untreated control mucosa and (B) In-situ lamotrigine gel - treated mucosa.